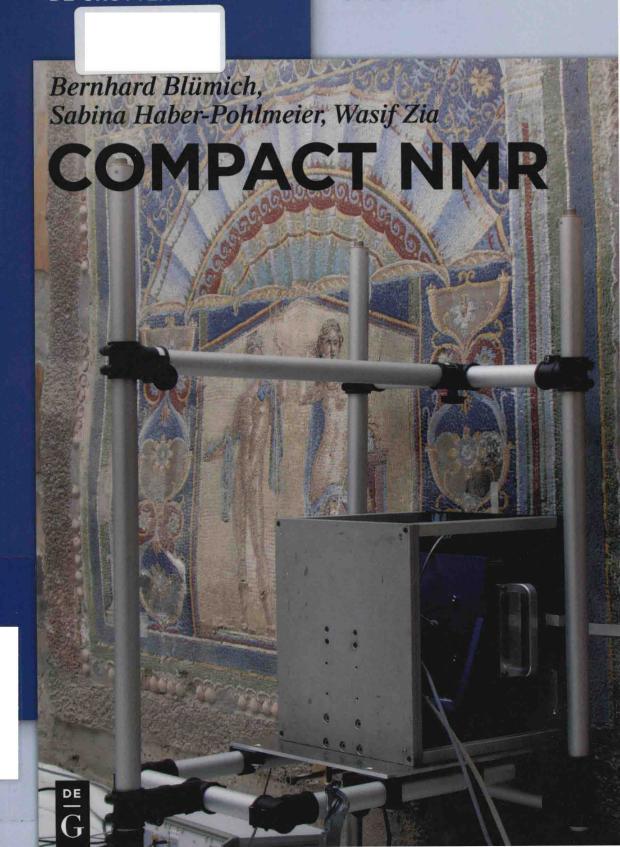
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Compact NMR



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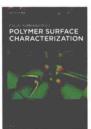
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Foreword

NMR is a complicated business. When we want to learn the trade, being fascinated by all these wonderful experiments the NMR experts tell us are simple to do, we get confronted with mountains of information about pulses, flip angles, the rotating coordinate frame, the density matrix, and more. How is it, that we cannot do NMR in the same manner as we are used to operating a DVD player or some other sophisticated technical gadget like a cell phone. Clearly, an NMR spectrometer is a bit more complicated than a coffee machine, and so the instructions for operating a spectrometer are not expected to be trivial. But is an NMR spectrometer really more complicated than a cell phone? Probably not! Nevertheless we can operate a mobile phone without knowing the technical details about its function and the electronics inside. So why can we not operate an NMR spectrometer and get decent results on a level of expertise similar to that required using a cell phone?

Today one of the most challenging tasks is the miniaturization of NMR machines for use as dedicated and personalized devices. Because the use of such compact devices is comparatively new and these NMR devices become more popular, this book intends to be a guide to their use and applications by providing the basic knowledge and operating instructions to perform successful NMR measurements. The content focuses on compact and mobile NMR machines for the analysis of materials and processes, because this technology is most likely to be in demand by investigators who have little to no knowledge about NMR. Following a basic introduction to NMR and compact NMR equipment in Chapter 1, the experimental set-up is discussed in Chapter 2. Several general types of NMR experiments are described in Chapter 3. Representative applications of these experiments to liquids, polymers, biological tissue, porous media, and objects from cultural heritage are collected in Chapters 4 to 8. For each case, a description of the measurement and data evaluation procedures is given with reference to the principles and procedures explained in the preceding chapters. Each description follows the same pattern including the objective, the theoretical background, the pulse sequences and parameters, beginners-level measurements, advanced-level measurements, and data processing. It is hoped, the information given will help the NMR novice to successfully conduct measurements with compact NMR equipment although it is not quite yet at the level of operating a cell phone.

This book has benefitted from the help of many friends and members of the Aachen NMR research group. They contributed earlier versions of some sections of the book, helped with proof reading, checked the pulse sequences and phase tables, and most importantly provided many of the experimental data given as examples in the text. We thank Alina Adams, Sophia Anferova, Vladimir Anferov, Stephan Appelt, Juliane Arnold, Maria Baias, Peter Blümler, Federico Casanova, Ernesto Danieli, Vasiliki Demas, Dan Demco, Gunnar Eidmann, Ralf Eymael, Stefan Glöggler, Nicolae Goga, Andreas Guthausen, Gisela Guthausen, Agnes Haber, Rolf Haken,

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Aachen, 31st August 2013

Bernhard Blümich Sabina Haber-Pohlmeier Wasif Zia

List of Symbols

| a_{fast} | amplitude of a rapidly decaying signal | $G_{ m phase}$ | phase-encoding gradient |
|---------------------------------|---|---------------------|--|
| | component | G_{read} | read gradient |
| $a_{\rm slow}$ | amplitude of a slowly decaying signal | $G_{\rm slice}$ | slice-selection gradient |
| | component | G_{χ} | <i>x</i> -component of the gradient vector |
| a_{ij} | component amplitudes | $G_{x,\max}$ | maximum gradient in x -direction |
| A | absorption signal, cross sectional area | h | hydraulic head, Planck's constant |
| b | power exponent in the Kohlrausch | ¹ H | hydrogen nucleus |
| | function | i | square root of -1 |
| b_1, b_2 | diffusion attenuation coefficient | J | water flow velocity |
| B | magnitude of the magnetic field | k | wave vector |
| \boldsymbol{B} | magnetic field vector | $k_{ m B}$ | Boltzmann constant |
| B_0 | magnitude of the homogeneous | k_{ij} | exchange rate |
| | magnetic field | k_{y} | wave number in y-direction |
| B_1 | amplitude of the radio-frequency | $k_{v,\text{max}}$ | maximum wave number in y-direction |
| | magnetic field | k_z | wave number in z-direction |
| \boldsymbol{B}_1 | vector of the rf magnetic field | $k_{z,\text{max}}$ | maximum wave number in z-direction |
| $oldsymbol{B}_{	ext{eff}}$ | effective field | K | matrix of exchange rates |
| $\boldsymbol{B}_{\mathrm{fic}}$ | fictive field | K | hydraulic conductivity |
| B_z | z-component of the magnetic field vector | K_{S} | hydraulic conductivity at full saturation |
| C | constant | $l_{\rm d}$ | diffusion length |
| C_1, C_2 | constants | ln | natural logarithm |
| C_{M} | spin-density contrast | log | logarithm of base 10 |
| $C_{\rm w}$ | contrast of the weight parameter, water | L | length |
| VV | capacity function | L_0 | initial length |
| dB | decibel | $m_{\rm s}$ | mass of solid phase |
| d_{i} | diameter of the interface domain | $m_{\rm t}$ | total mass |
| d_{m} | diameter of the mobile domain | $m_{\rm w}$ | mass of water phase |
| $d_{\rm r}$ | diameter of the rigid domain | M | nuclear magnetization vector |
| D | diffusion coefficient, dispersion signal, | $M_{\rm O}$ | thermodynamic equilibrium |
| _ | soil water diffusivity | ****0 | magnetization, spin density |
| D_0 | self-diffusion coefficient of the pure | $M_{ m Oref}$ | spin density of a reference compound |
| 20 | substance | M_2 | second moment |
| D cc | effective diffusion coefficient | M(t) | complex transverse magnetization |
| $D_{ m eff}$ exp | exponential function | $M_{\rm c}$ | molecular weight between cross-links |
| E | energy | IVI C | in an elastomer |
| | energy of spins pointing up | $M_{\rm p}$ | number-average molecular weight |
| E_{\uparrow} | energy of spins pointing dp | 55.000 | component of the magnetization |
| $\frac{E_{\downarrow}}{f}$ | scaling factor | M_{χ} | vector in x-direction |
| FT | Fourier transformation | M_{y} | component of the magnetization |
| G | magnitude of the magnetic field | IVI y | vector in y-direction |
| U | gradient, shear modulus | M | |
| G | magnetic field gradient vector | M_z | component of the magnetization vector in <i>z</i> -direction |
| | effective field gradient | n | number, cross-link density, |
| $G_{ m eff}$ | internal field gradient | n | |
| $G_{\rm int}$ | | n | van Genuchten parameter |
| G_{\max} | maximum gradient value | n_{\uparrow} | number of spins pointing up |

| n_{\downarrow} | number of spins pointing down | T | absolute temperature |
|---------------------|--|-----------------------|--|
| n_1, n_2 | numbers | TX | transmitter |
| n_{acq} | number of acquired data points | T_1 | longitudinal relaxation time |
| $n_{\rm E}$ | number of echoes | $1/T_1$ | longitudinal relaxation rate |
| $n_{\rm f,max}$ | maximum number of frequency | $1/T_{2}$ | transverse relaxation rate |
| | encoding steps | $1/T_{1\text{bulk}}$ | longitudinal relaxation rate of the bulk |
| n_{G} | number of gradient steps | $1/T_{2bulk}$ | transverse relaxation rate of the bulk |
| $n_{p,max}$ | maximum number of phase encoding | $1/T_{2diff}$ | transverse relaxation rate for |
| | steps | | diffusion in gradients |
| $n_{\rm s}$ | number of scans | $1/T_{2surf}$ | surface transverse relaxation rate |
| p | Laplace variable | T_0 | time constant |
| P | probability density | T_{10} | longitudinal relaxation time of the |
| P(r) | droplet size distribution | | oil phase |
| q | fraction | T_{1w} | longitudinal relaxation time of the |
| Q | volume flow rate | | water phase |
| r | radius, magnitude of space vector | T_2 | transverse relaxation time in |
| r | space vector | | homogeneous field |
| $\langle r \rangle$ | mean radius | T_2^* | transverse relaxation time including |
| R | ideal gas constant, constant, | | field inhomogeneity |
| | magnitude of the displacement vector, | T_{2A} | transverse relaxation time of |
| | hydrodynamic radius | | component A |
| R | relaxation matrix | T_{2B} | T ₂ of component B |
| RX | receiver | T_{2C} | T ₂ of component C |
| S | signal | T _{2bulk} | transverse relaxation time of the bulk |
| s_{2Q} | double quantum signal | $T_{2\mathrm{eff}}$ | effective transverse relaxation time |
| $s_{\rm d}$ | signal of a distribution | $T_{\text{2eff,0}}$ | reference effective transverse |
| S_{ref} | reference signal | 2011,0 | relaxation time |
| S | spectrum, Fourier transform of s, | Tacff anico | anisotropic T_{2eff} |
| | surface area | | T_{2eff} of the interfacial component |
| SFC | solid fat content | $T_{\text{2eff,iso}}$ | isotropic T_{2eff} |
| t | time | | T_{2eff} of the mobile component |
| | acquisition time | | T_{2eff} of the rigid component |
| t_{acq} | dead time | $T_{\rm 2lm}$ | logarithmic mean value of the |
| $t_{\rm d}$ | echo time, dito t_{E1} , t_{E2} , t_{E2} | ¹ 2lm | relaxation distribution |
| $t_{\rm E}$ | effective echo time | T | long relaxation time |
| $t_{\rm E,eff}$ | filter time | T _{2long} | short relaxation time |
| $t_{\rm f}$ | | T _{2short} | real part of the NMR signal recorded |
| $t_{\rm m}$ | mixing time multiquantum evolution time | и | in the time domain |
| t _{MQ} | | U | real part of the spectrum |
| t _p | pulse width duration of $G_{\rm phase}$ | | imaginary part of the NMR signal |
| t _{phase} | duration of G_{phase} | ν | recorded in the time domain |
| t _{read} | repetition time, recycle delay | V | imaginary part of the spectrum, |
| $t_{\rm R}$ | | V | volume |
| t_z | storage time for a longitudinal | T/ | A ALEXANDER |
| | magnetization | $V_{\rm g}$ | volume of gas phase |
| t_0 | recovery time | $V_{\rm s}$ | volume of solid phase |
| t_1 | evolution time, evolution period | $V_{\rm t}$ | total volume |
| t_2 | detection time, detection period | $V_{\rm w}$ | volume of water phase |
| t ₉₀ | duration of the 90° pulse | W | weight parameter, relaxation- |
| t_{180} | duration of the 180° pulse | | weighted spin density |
| | | | |

| x, y, z | space coordinates | η | viscosity |
|----------------------------------|---|-------------------------------|---|
| x, y, z | unit vectors along the Cartesian | ĸ | fluid permeablity |
| , , , | space coordinates | Λ | elongation ratio |
| x_{A} | number fraction of component A, | ν | frequency in Hz |
| A | crystallinity | v_0 | Larmor or precession frequency in Hz |
| $x_{\rm B}$ | number fraction of component B | v_{max} | maximum frequency |
| X _C | number fraction of component C | $v_{\rm max}$ | reference frequency |
| X_i | number fraction of the interfacial | v_{rf} | NMR frequency for transmitter and |
| ~1 | component | •п | receiver in Hz |
| $x_{\rm m}$ | number fraction of the mobile | θ_{m} | water content of mass fraction |
| 111 | component | $\theta_{\rm r}$ | bound water content |
| x_{max} | field of view in <i>x</i> -direction | $\theta_{\rm V}$ | volumetric water content |
| X _r | number fraction of the rigid | Θ | normalized water saturation |
| -1 | component | Θ_{S} | water saturation |
| z_{max} | field of view in z-direction | ω | frequency in rad/s |
| α | flip angle of an rf pulse, | ω_0 | Larmor frequency in rad/s |
| 54 | van Genuchten parameter | ω_1 | nutation frequency in rad/s |
| $\alpha_{\rm E}$ | Ernst angle | $\omega_{\rm f}$ | final frequency in rad/s |
| У | gyromagnetic ratio | ω_i | initial frequency in rad/s |
| Δ | diffusion time | $\omega_{\rm rf}$ | NMR frequency for transmitter and |
| $\Delta G_{\rm phase}$ | increment of G_{phase} | П | receiver in rad per second |
| ΔG_z | increment of gradient in z-direction | Ω | frequency offset from the rf |
| Δt | dwell time, sampling interval | | transmitter frequency |
| Δt_1 | increment of the evolution time | π | half the circumference of the unit circle |
| $\Delta t_{\rm F}$ | increment of the echo time | ϖ_{D} | residual dipole-dipole interaction |
| $1/\Delta x$ | spatial resolution in <i>x</i> -direction | θ | polar angle |
| Δф | phase increment | ρ | density |
| $\Delta v_{1/2}$ | line width in Hz | | surface relaxivities |
| | line width in rad/s | $\rho_{1,2}$ | density of solid particles |
| $\Delta\omega_{1/2}$ | chemical shift, duration of a gradient | $\rho_{\rm s}$ $\rho_{\rm t}$ | density of bulk soil |
| U | pulse | σ | standard deviation |
| δ_{max} | maximum chemical shift | τ | delay between the first and the |
| € | strain | | second pulse in an echo sequence |
| φ | precession angle | $\tau_{\rm c}$ | correlation time of molecular motion |
| 100 | transmitter phase of pulse 1 | | exchange time between sites <i>i</i> and <i>j</i> |
| φ_1 | receiver phase for data acquisition | $τ_{ij}$ ψ | total water potential |
| φ _{acq} | receiver phase | Ψ_{m} | matrix potential |
| φ _{RX} | transmitter phase | $\Psi_{\rm m}$ $\Psi_{\rm o}$ | osmotic potential |
| φ _{TX} φ | phase error | $\Psi_{\rm p}$ | additional air pressure potential |
| φ Φ ₀ | constant phase correction parameter | Ψ_p Ψ_z | gravitational potential |
| Ψ ₀ Φ ₁ | linear phase correction parameter | $Ψ_z$ $Ψ_H$ | hydraulic potential |
| Ф1 | porosity | ΨH $Ψ$ Ω | overburden potential |
| 190 | potosity | $\Phi\Omega$ | overburden potential |

List of Acronyms

| 1D | one-dimensional | MIP | Mercury Intrusion Porosimetry |
|-------------|---|--------------|-----------------------------------|
| 2D | two-dimensional | MOUSE | Mobile Universal Surface Explorer |
| 2Q | double quantum | MRI | Magnetic Resonance Imaging |
| 3D | three-dimensional | MRT | Magnetic Resonance Tomography |
| ADC | Analog-to-Digital Converter | MQ | MultiQuantum |
| AOCS | American Oil Chemists' Society | NMR | Nuclear Magnetic Resonance |
| ASCII | Amercian Standard Code for Information | NOESY | Nuclear Overhauser Effect |
| | Interchange | | SpectroscopY |
| CLI | Command Line Interface | o/w | oil-in-water |
| COSY | COrrelation SpectroscopY | PE | PolyEthylene |
| CPMG | Carr, Purcell, Meiboom, Gill | PFG | Pulsed Field Gradient |
| C-S-H | calcium silicate hydrate | Prospa | Processing package |
| CT | Computer Tomography | PVC | PolyVinylChloride |
| CUFF | Cut-open, Uniform, Force Free | PTFE | PolyTetraFluoroEthylene |
| CYCLOPS | S CYClically Ordered Phase Sequence | rf | radio frequency |
| DOSY | Diffusion Ordered SpectroscopY | RARE | Rapid Acquisition with Relaxation |
| EXSY | EXchange SpectroscopY | | Enhancement |
| FID | Free Induction Decay | RMS | Root Mean Square |
| FLASH | Fast Low Angle Shot | ROSY | Relaxation Ordered Spectoscopy |
| FSP | Fiber Saturation Point | RPA | Rubber Process Analyzer |
| FT | Fourier Transformation | RX | Receiver |
| GARfield | Gradient At Right angle to the magnetic | SEC | Size-Exclusion Chromatography |
| | field | SFC | Solid Fat Content |
| GPC | Gel Permeation Chromatography | SNR | Signal-to-Noise Ratio |
| HetCor | Hetero-nuclear Correlation | SPAC | Soil Plant Atmosphere Continuum |
| HDPE | High-Density PolyEthylene | S/V | Surface-to-Volume ratio |
| IR | InfraRed | SQUID | Superconducting Quantum |
| ISO | International Organization for | | Interference Device |
| | Standardization | TX | Transmitter |
| LDPE | Low-Density PolyEthylene | USB | Universal Serial Bus |
| LLDPE | Linear Low-Density PolyEthylene | UV | Ultra Violet |
| ln | logarithmus naturalis | w/c | water/cement ratio |
| MAS | Magic Angle Spinning | w/o | water-in-oil |

and particles of

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1 Introduction to NMR

The chemist calls it *NMR* and the medical doctor *MRI*. *Nuclear magnetic resonance* (NMR) is the most popular tool in chemistry to analyze molecular structures, and *magnetic resonance imaging* (MRI) is a non-invasive diagnostic tool in the hospital that provides high-contrast *images* of tissues depicting the brain functions and the beating heart. In both cases large and expensive superconducting magnets are employed (Fig. 1.0.1), which magnetize the object by aligning the atomic nuclei inside the magnet. The resulting magnetization can be triggered by radio frequency waves to rotate around the direction of the magnetic field. Depending on the operating mode, the frequency *spectrum* of the rotating nuclear magnetization provides the chemist with molecular information and the medical doctor with anatomical images, while the materials scientist may be interested in the decay of the *impulse response* to learn about physical properties of a solid object like a wet wall.

1.1 NMR: Nuclear Magnetic Resonance

NMR can be defined as a physical phenomenon which is utilized to investigate molecular properties of matter by irradiating atomic nuclei in a *magnetic field* with electromagnetic *radio waves*. Many nuclear isotopes possess an angular momentum called *spin*. In classical terms, spins appear to rotate around an axis like a bicycle wheel (Fig. 1.1.2a). For atomic nuclei, however, the somewhat unusual laws of *quantum mechanics* apply. For example, every spin is associated with a *magnetic moment* like the





Figure 1.0.1. High-field NMR machines with superconducting magnets and compact, low-field machines with permanent magnets (insets). (a) Magnets for chemical analysis. (b) Magnets for magnetic resonance imaging (MRI). The patient or the object is positioned in the center of the magnet hole. The bulky electronics of medical MRI machines are typically hidden in a separate room.

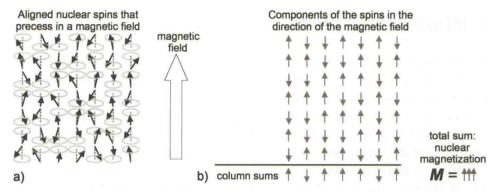


Figure 1.1.1. Schematic drawing of 49 out of 10^{23} proton spins which are aligned in a magnetic field. (a) Each spin appears to rotate or 'precess' around the direction of the magnetic field in a manner similar to a spinning bicycle wheel, which precesses around the direction of the gravitational field (Fig. 1.1.2a). (b) The up and down states of the spins are more easily recognized when only the part of the spin vector parallel to the direction of the magnetic field is drawn. Because each spin is a magnet, each of these arrows represents a magnet. The nuclear magnetization M is the sum of the magnetizations from each component magnet.

needle of a compass. Depending on the magnitude of the spin, it can align with a magnetic field in different stable orientations, which differ in their inclination angles with respect to the magnetic field and therefore also differ in their energies (Fig. 1.1.1a). *Protons*, the most abundant nuclear spins in organic matter, align in two states, called up (\uparrow) and down (\downarrow). The relative numbers n_{\uparrow} and n_{\downarrow} of spins for the two states with energies E_{\uparrow} and E_{\downarrow} follow the *Boltzmann distribution*, where $k_{\rm B}$ is the Boltzmann constant and T is the temperature in Kelvin,

$$\frac{n_{\downarrow}}{n_{\uparrow}} = \exp\{-(E_{\downarrow} - E_{\uparrow})/(k_{\rm B}T)\}. \tag{1.1.1}$$

The *nuclear magnetization* M of a macroscopic sample with some 10^{23} spins is formed by the difference $n_1 - n_1$ of the number of spins with different orientations (Fig. 1.1.1b).

Because the resulting magnetization M is composed of an unimaginably large number of quantum mechanical entities, it behaves like a classical magnet, which spins around its magnetization axis. It interacts with a magnetic field B_0 in the same way as a gyroscope e.g., in the way a spinning bicycle wheel interacts with the gravitational field (Fig. 1.1.2a): When not aligned with the direction of the field, the magnetization axis rotates around the direction of the field (Fig. 1.1.2b). This rotation is called precession. The precession frequency or Larmor frequency ω_0 is proportional to the strength B_0 of the applied field,

$$\omega_0 = 2\pi \nu_0 = \gamma B_0 \tag{1.1.2}$$

where the *gyromagnetic ratio* γ is a constant specific to the type of atomic nucleus, and $\nu_0 = (E_{\downarrow} - E_{\uparrow})/h$, where h is Planck's constant. For example, the frequency ν_0 for